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Published in:
Journal of Nuclear Medicine

DOI:
[10.2967/jnumed.120.256230](https://doi.org/10.2967/jnumed.120.256230)

Publication date:
2021

Document Version
Peer reviewed version

[Link to publication in Discovery Research Portal](#)

Citation for published version (APA):

Zhang, X., Landgraf, L., Bailis, N., Unger, M., Jochimsen, T. H., & Melzer, A. (2021). Image-Guided High-Intensity Focused Ultrasound, A Novel Application for Interventional Nuclear Medicine? *Journal of Nuclear Medicine*, 62(9), 1181-1188. <https://doi.org/10.2967/jnumed.120.256230>

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Image-guided High-Intensity Focused Ultrasound, A Novel Application for Interventional Nuclear Medicine?

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ABSTRACT

Image-guided high-intensity focused ultrasound (HIFU) has been increasingly used in medicine over the past few decades, and several systems for such have become commercially available. HIFU has passed regulatory approval for the ablation of various solid tumors, the treatment of neurological diseases, and the palliative management of bone metastases around the world. The mechanical and thermal effects of focused ultrasound provide a possibility for histotripsy, support radiation therapy, and targeted drug delivery. The integration of imaging modalities into HIFU systems allows for precise temperature monitoring and accurate treatment planning, increasing the safety and efficiency of treatment. Preclinical and clinical results have demonstrated the potential of image-guided HIFU to reduce adverse effects and increase the quality of life postoperatively. Interventional nuclear image-guided HIFU is an attractive noninvasive option for the future.

Keywords: image-guided HIFU; targeted drug delivery; tumor ablation; hyperthermia; PETMR image-guidance

INTRODUCTION

High-intensity focused ultrasound (HIFU) has gained clinical acceptance for therapeutic applications, especially as a thermal ablative treatment modality for benign uterine fibroids, bone metastases, and prostate carcinoma as well as for essential and Parkinson's tremors (1). HIFU ablation at temperatures above 55 °C is considered noninvasive surgery without physical access to the target region, and clinical HIFU systems have received regulatory approval in Europe, America, and Asia (2). Additionally, HIFU-induced hyperthermia in a temperature range of 40–45 °C for up to 60 min was reported as a sensitizer for ionizing radiation and a mediator of thermal-sensitive drug delivery in the treatment of solid tumors (3).

Compared with other clinically used techniques for thermal therapy (ablation) such as laser, radiofrequency, and microwaves, which generate heat through probes by electromagnetic waves, causing the rotation of water molecules and thus inducing heating, ultrasound is a mechanical-wave-based technique. Although it is possible to generate focused heat through microwaves or radiofrequencies, electromagnetic waves cannot be focused as precisely as ultrasound waves, and the penetration depth of electromagnetic waves is limited. HIFU provides adequate tissue penetration, ranging from 1 to 20 cm, with specific focal spot. Therefore, it overcomes the limitation of electromagnetic wave-based techniques. Moreover, HIFU is a promising alternative and the only noninvasive technique for clinical ablation and hyperthermia (4).

In recent years, image-guided therapeutic interventions have become an increasingly important area in oncology field, integrating radiological imaging methods, e.g. magnetic resonance (MR) imaging, ultrasound imaging, computed tomography (CT), X-ray, and positron emission tomography (PET), with surgery and therapies (2). Evaluation of treatment with an adequate imaging protocol is essential as a clinical prognostic readout. The broad clinical applications of HIFU were reviewed by Izadifar *et al.* (5). In addition to that, we provide clinical details of some of the most prevalent and important clinical HIFU applications, describing the relative systems for these clinical cases. An overview of the latest preclinical and clinical studies is given in this review.

PRINCIPLES OF HIFU

Regarding the application of HIFU, ultrasound waves are typically generated by piezoelectric material, and focusing is enabled either by a single focused transducer that bundles sound waves with the bowl-shape transducer (Figure 1A) or by phased array transducers via beamforming (Figure 1B).

Numerous parameters should be taken into consideration from the physical aspect. For example, the selected frequency, in the range of 0.25–3 MHz for medical applications, is related to penetration depth, indications, and the required acoustic intensity. For intra-abdominal applications, the frequency of 1 MHz is typically used to produce sufficiently high intensities for deep-seated tissues. Another important parameter is the acoustic impedance, which is composed of sound speed in the medium and the density of the medium, affecting the transport of sound waves. When ultrasound waves propagate through tissues, sound waves are reflected at the interface if the acoustic impedances of two tissues are different. The reflection of sound waves can increase the signal display and help to distinguish the tissue interface (e.g., muscle and bone interface) with diagnostic ultrasound; however, it is unexpected and may cause injuries in HIFU applications. Thus, air bubble-free coupling of the patient to the HIFU system is required to avoid reflection-induced skin damage. In this context, image-guidance is of high importance to prevent scattering or the reflection of sound waves and avoid potential safety issues, especially for applications close to specific regions such as the lungs, intestines, and bones (6).

HIFU generates acoustic waves at a high energy level; the absorption of acoustic energy creates thermal effect in the tissues via mechanical friction. Cavitation, acoustic radiation force, acoustic streaming, and shock waves are considered non-thermal mechanisms of HIFU-induced biological effects. Cavitation describes the oscillation and collapse of gas-filled cavities in the acoustic field. The process is divided into stable (non-inertial) and inertial cavitation (7). Enhanced membrane permeability via the induction of stable cavitation is named sonoporation, and this is applied for blood–brain barrier opening and the support of drug delivery into the central nervous system. In contrast, inertial cavitation is typically used for tissue destruction (histotripsy) or in combination with chemotherapy, which is the so-called sonodynamic therapy (8).

Histotripsy describes the disintegration or liquefaction of tissue by short ultrasound shots, showing that HIFU is capable of generating pure mechanical damage to tissues (Figure 1C).

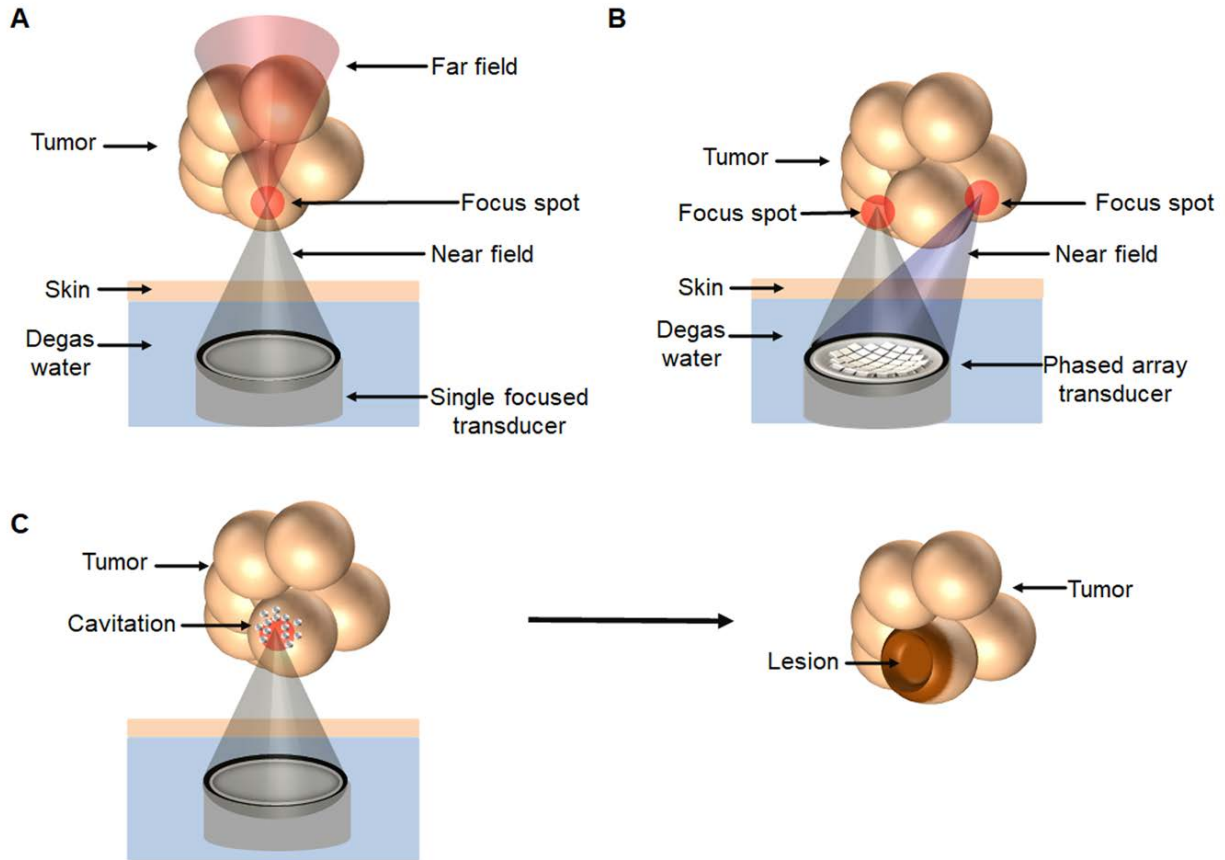


FIGURE 1. Schematic representation of high-intensity focused ultrasound (HIFU) ablation. **A** The high level of sound energy in the focal spot leads to heating of the tissue to temperatures above 55 °C, resulting coagulation with subsequent necrosis in tissue. Sensitive structures in the near and far fields can be spared. **B** Ablation of large volume tumors is realized by scanning the focal zone through the entire tumor using a phased array transducer via beamforming. **C** Histotripsy destroys the tissue by the induction of cavitation events generating lesions in the target region.

IMAGING GUIDANCE MODALITIES AND THERMOMETRY

To ensure the noninvasiveness of HIFU application, imaging guidance plays essential roles in treatment planning, temperature monitoring and follow-up after therapy. Currently, only single-modality

imaging guidance, either ultrasound imaging or MR imaging, is used in clinic. Dual-modality imaging, such as PET-CT and PET/MRI, has drawn attention in recent years. Integration of the HIFU system into PET/MRI provides additional information of metabolism in the targeted tissue and allows “precise HIFU-triggered drug delivery”, especially for the treatment of neurodegenerative diseases.

Ultrasound imaging enables real-time anatomic imaging during HIFU treatment, offering an advantage for the treatment of moving organs. For example, tumor in the liver moves together with respiration during treatment and may lead to noise in MR images, but ultrasound imaging can overcome such limitations (9). The main drawback of ultrasound imaging-guided HIFU (USgHIFU) is the lack of real-time temperature mapping, the temperature and the thermal dose inside the target region cannot be determined. Since temperature feedback to control ultrasound power is not available, USgHIFU is usually conducted using a short sonication duration (e.g., 3–4 s) to avoid overheating and may result in incomplete ablation (10). Moreover, the high absorption and reflection of ultrasound by the skull bone are the main limitations of transcranial ultrasound and restrict the treatment of neurological diseases using USgHIFU.

In contrast, MR imaging-guided HIFU (MRgHIFU) provides spatial guidance in the targeted area for precise treatment planning. Near real-time temperature monitoring during treatment is feasible via MR thermometry using temperature-dependent proton resonance frequency shift, T1 temperature mapping, or diffusion temperature mapping (11). However, MRgHIFU is more costly than USgHIFU, and the patient is required to be enclosed in a confined MR scanner during treatment.

CLINICAL APPLICATIONS OF IMAGE-GUIDED HIFU

Image-guided HIFU systems have been developed and are used clinically for the treatment of various diseases. Based on physical parameters and available clinical systems with a focused spot of 1 mm–4 cm (5), HIFU treatment is typically conducted through several subsequential sonications (refers to the application of ultrasound energy) across the whole treated region. Here, we discuss some of the most commonly used clinical applications and relevant HIFU systems. Commercially available clinical HIFU systems are listed in Table 1.

Ablation of Uterine Fibroids

Uterine fibroids are the most common benign tumors in the uterus, showing great variability in terms of shape, size, and localization. They occur in up to 80% of women during the reproductive period and are the leading indication for hysterectomy. Clinically relevant symptoms, including pelvic pain, dysmenorrhea, and dyspareunia, can be relieved with pharmacological agents; however, adverse effects and a lack of adequate control are the main problems. Hospitalization and several weeks of recovery time are required after surgical resection (12).

The MRgHIFU system ExAblate 2000 (INSIGHTEC, Israel) was first approved by U.S. Food and Drug Administration to treat uterine fibroids in 2004, and Sonalleve system from Profound Medical was approved in Europe in 2011 (Figure 2A). The Sonalleve system is introduced as an example. The phased-array transducer consists of 256 elements that can be controlled independently, allowing “beamforming”. Formation of the ultrasound beam is established through electronic activation of each element separately at different phases, thereby creating a target zone with variable sizes and orientations. The treatment is planned based on the T2-weighted MR image, and the treatment volume within the target fibroids is determined in three orthogonal planes. Each sonication increases the temperature to 60–85 °C in a matter of seconds and causes coagulative necrosis. The treatment outcome is evaluated with the nonperfused volume (NPV) via contrast-media-supported T1 images (Figure 2B). NPV describes the tissue volume without blood flow and is correlated with a fibroid volume reduction. In most cases, only a few hours of clinical monitoring is necessary, and the patients can continue with their daily activities after HIFU treatment.

Compared with traditional surgery, HIFU treatment is less invasive, avoids general anesthesia, and has the advantages of low morbidity, fewer complications, and shorter recovery time. The symptoms almost or entirely subside 3–12 months after successful therapy (NPV>60%). Various studies have shown a reduction in fibroid-associated complaints and an improved quality of life. The most significant advantage of image-guided HIFU over myomectomy is the higher pregnancy rate and the significant reduction in the time interval between pregnancy and treatment. The incidence of uterine rupture is rare in pregnant patients

who have received HIFU ablation previously but should be considered to avoid serious adverse effects (13). The disadvantages are limited to the relatively long treatment duration of 2–4 hours and the latency period to freedom from symptoms. Notably, the thickness of abdominal subcutaneous fat and the abdominal scar are associated with thermal injury and influence the risk of unsuccessful HIFU ablation of uterine fibroids (14). This complication can be avoided by careful preparation of the patients.

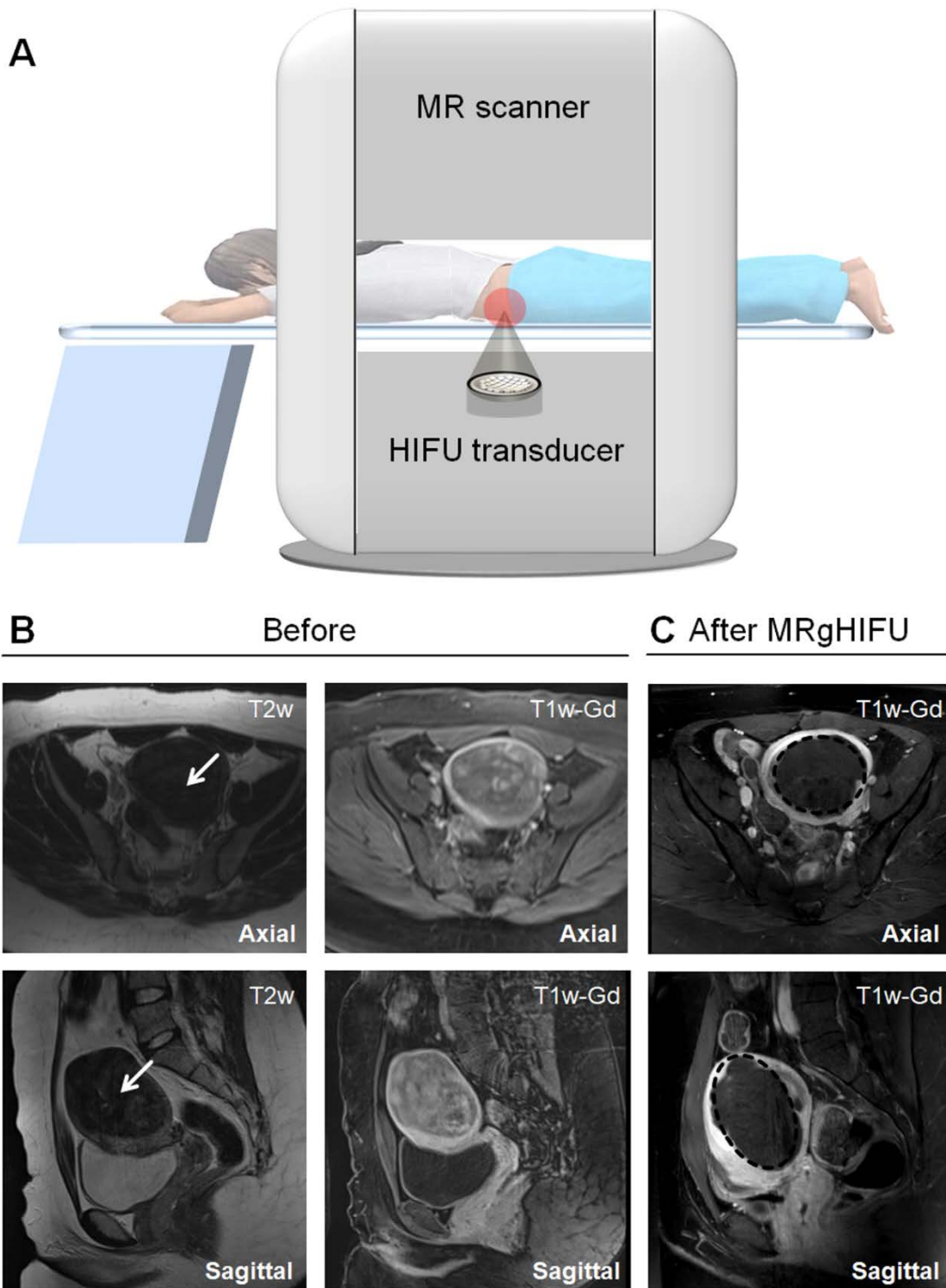


FIGURE 2. Magnetic resonance imaging-guided HIFU (MRgHIFU) for uterine fibroid treatment. **A** Schematic drawing of MRgHIFU treatment of uterine fibroids with the Sonalleve (Profound Medical) or ExAblate 2000 (INSIGHTEC). Diagnostic T2-weighted and T1-weighted contrast-enhanced (Gd) images

of patients with hyper- and dysmenorrhea and Funaki Type 1 fibroid before (**B**, white arrow) and after MRgHIFU (**C**, black circle). Fibroid volume: 184 mL; treatment duration: up to 4 h.

Ablation Treatment of Essential Tremors

Essential tremor is a neurological disorder that causes rhythmic shaking, most often in hands, and has a great impact on the quality of life. Some patients may not be able to work due to uncontrolled movements (15). Medications can be used at the early stage but are insufficient when the tremor progresses. Surgery is highly effective; however, open neurosurgical operation is associated with risks such as serious neurological deficits and infections.

The ExAblate Neuro system from INSIGHTEC (Figure 3A), compatible with both GE and Siemens MR scanners, has been approved for the treatment of essential and Parkinson's tremors and pain treatment. The helmet-shaped phased array transducer contains 1024 individual elements, enabling the focus of ultrasound beams in deep brain targets without a surgical incision. A sealed degassed water system is used for coupling and cooling during treatment. Clinical systems for the blood–brain barrier opening operate at 250 kHz, and systems for ablation while penetrating the skull operate at 720 kHz. The frequencies used for neurological applications are lower than those used for body applications.

A pivotal clinical trial, conducted at eight international centers for the treatment of essential tremors using the ExAblate transcranial MRgHIFU system (NCT01827904), is in the final phase of a 5-year follow-up. Improvement of the hand-tremor score was observed three months after treatment (16), and continued beneficial effects in tremor control and the quality of life were reported with no progressive complications in the follow-up up to 4 years (17).

Ablation of Thyroid Nodules and Breast Fibroadenomas

Thyroid nodules are common and are mostly benign, although some become large and symptomatic (18). Surgical resection is the standard treatment, but may cause bleeding, hematoma, and infection, and

general anesthesia is required. HIFU allows non-surgical ablation and offers an alternative treatment for benign thyroid nodules (19).

To date, the EchoPulse® (THERACLION, France, Figure 3B) is the only commercially available device for the treatment of thyroid nodules. It consists of an ultrasound imaging system and a HIFU delivery system. The linear array imaging probe uses frequencies of 7.5–12 MHz as guidance, and the treatment is performed with the HIFU probe at 3 MHz with an acoustic power of up to 125 W.

The first-in-human trial of the HIFU ablation of thyroid nodules was performed in France (20). The pathological analysis showed significant nodule destruction, and histological examination demonstrated that ablated lesions were confined to the target region without damage to surrounding tissues. The safety and efficiency of the treatment were confirmed by Prakash *et al.* (21). The diameters of the thyroid nodules were reduced at 6 months post-treatment without complications (e.g., skin burn and hematoma), demonstrating the great potential of HIFU in the treatment of thyroid nodules.

In addition, breast fibroadenoma is another indication that can be treated using the EchoPulse® system. A clinical trial was conducted where patients were treated at intensity of 40 W for 38 min under local anesthesia, a success rate of 89% was reported (22).

Ablation of Prostate Cancer

Prostate cancer is the second-most-common cancer in men worldwide (23). Conventional clinical therapies such as hormone therapy (chemical castration), radiation therapy, and prostatectomy have side effects including loss of sexual function, injury of the neurovascular bundle, and induction of urinary incontinence. Hence, a local treatment option is gaining increasing interest. Laser ablation, cryoablation, and irreversible electroporation are used for prostate ablation (24), all of these applications require the insertion of probes with associated side effects.

As the first approved MRgHIFU system for prostate cancer ablation, the TUSLA-Pro system (Figure 3C) developed by Profound Medical (Canada) combines real-time MR imaging and robotically-

driven transurethral ultrasound with temperature control. The individually controlled elements in the transurethral applicator generate directional thermal ultrasound, and an endorectal water-cooling device protects the rectum during treatment. The treated prostate tumor volume is limited to 40 cc for most of the transrectal HIFU systems, a total ablation of larger volumes is difficult due to the limited penetration depth. In contrast, the transurethral applicator has advantages for ablation of prostate lesions up to 200 cc by continuous rotation. The TUSLA-Pro system can be integrated into MR scanners from various vendors, clinical feasibility and safety have been proven (25). The first integration with the PET/MRI scanner at OncoRay, University Dresden, Germany was realized within our SonoRay BMBF Project (<https://www.oncoray.de/research/sono-ray>), and a pilot clinical study is being conducted.

A multi-center Phase I clinical trial of MRgHIFU whole-gland prostate ablation (NCT01686958) was conducted using the TUSLA-Pro system, and the radiological findings were reported by Bonekamp et al. (26). Chin *et al.* (27) reported the oncological outcomes and quality of life, and stated that the erectile function of the patients was recovered after 12 months. Klotz et al. (28) reported similar outcomes from a prospective trial (NCT02766543) with 115 patients in 2021, whereby the prostate-specific antigen decreased in 96% of the patients, and erections were maintained in 75% of the patients after 12 months. The clinical data suggest that TUSLA-Pro is an effective tool for prostate cancer ablation with minimal impact on the quality of life.

The novel HIFU hemiablation procedure targets only the cancerous tissue of the prostate, enabling the healthy tissue to be spared, which shows the potential to increase the effectiveness and safety of treatment compared with the entire gland resection. Ganzer et al. (29) reported a multi-center phase II trial using the HIFU hemiablation approach. The one-year follow-up indicated a significant reduction in the prostate-specific antigen from 6.2 to 2.9 ng/ml. Patients had a preserved quality of life after treatment. The lack of long-term follow-up on oncological control and functional outcomes is the main obstacle to encouraging patients to choose this approach.

Pain Relief of Bone Metastases

Bone is a common site of solid tumor metastases. Symptoms, including localized pain, pathological fractures, and functional deficits, may occur early in the metastatic course. The treatment of painful metastases requires an interdisciplinary approach involving different clinical disciplines. There are many procedures available for treatment. The most common method is radiotherapy at a single fraction of 8 Gy or 30 Gy in 10 fractions; however, a high toxicity rate was reported (30).

In a Phase III study (31), pain relief was observed in two-thirds of the respondents within three days after MRgHIFU treatment. Similarly, 89% of the patients experienced a pain reduction, 72% of whom were completely pain-free, as reported by Napoli *et al.* (32). These results highlight the capability of HIFU in pain management of bone metastases with rapid, successful, and durable effects. A new multi-center, three-armed, randomized control trial, including more than 200 patients, started in 2020 to investigate the pain palliation effect of MRgHIFU as an alternative or addition to radiotherapy (NCT04307914).

For a successful HIFU treatment, patient selection is critical. Lesions of the spinal column should be carefully assessed because of the adjacent critical nerve structures. Notably, blood perfusion in highly vascularized lesions will lead to a heat-sink effect, and embolization should be considered in these cases.

Ablation of Pancreatic Cancer

Pancreatic cancer is aggressive with a poor 5-year survival rate of 8%. Symptoms include jaundice, malaise, weight loss, and loss of appetite, reducing patients' quality of life severely. Cancer-related abdominal or back pain is experienced in most patients, while established chemotherapy or radiochemotherapy have limited anti-tumor effects and pain control durations (33).

The most frequently used clinical USgHIFU system "JC" was developed by HAIFU (Chongqing, China, Figure 3D) and has been approved for the treatment of uterine fibroids, pancreatic cancer, and liver, bone, and breast tumors. The system has a 0.8 MHz single transducer integrated into the patient table, and fronted acoustic lenses allow focus length adjustment. An ultrasound-imaging device (1–8 MHz) is equipped for real-time guidance.

A clinical trial in 2018 showed a reduction in tumor volume of 58% after 6 months and a longer median overall survival (16.2 months) compared with patients who received chemotherapy/radiochemotherapy (34). An improvement in quality of life was reported in 2021, where physical, emotional, and social functioning increased with a low rate of side effects, demonstrating that HIFU is a worthwhile supportive treatment for advanced pancreatic cancer (35).

Table1 Clinical used HIFU systems

Clinical MR imaging-guided HIFU (MRgHIFU) systems			
Device	Company	Location	Application field
Low Intensity Focused Ultrasound Pulsation (LIFUP)	BrainSonix	Sherman Oaks, California	Neuromodulation
Sonalleve TULSA-PRO	Profound Medical Inc.	Mississauga, Canada	Myomas, Bone metastasis, Prostate carcinoma
SonoCloud®	CarThera	Paris, France	Brain
TargetedFUS	Image Guided Therapy	Pessac, France	Breast, Uterus
ExAblate 2000	INSIGHTEC® LTD	Tirat Carmel, Israel	Uterus
ExAblate 4000			Essential Tremor
ExAblate 2100 CBS			Bones
ExAblate Prostate			Prostate
ArcBLATE	EpiSonica	Hsichu City, Taiwan	Uterus, Pancreas
Clinical ultrasound imaging-guided HIFU (USgHIFU) systems			
Device	Company	Location	Application field
Edison	HistoSonics, Inc.	Ann Arbor, Michigan, USA	Prostate
ICC HIFU Synthesizer	International Cardio Corporation, LLC	Minnetonka, Minnesota, USA	Arteriosclerosis
Mirabilis	Mirabilis Medical	Bothell, Washington, USA	Uterus Fibroids
Sonablate	SonaCare Medical, LLC	Charlotte, North Carolina, USA	Prostate
Valvopulse	Cardiawave	Paris, France	Aortic valve stenosis
ECHOPULSE	Theraclion	Malakoff, France	Fibroadema breast, Thyroid
ALPIUS 900	Alpinion Medical Systems	Seoul, Korea	Uterus
FEP-BY02	Beijing Yuande Bio-Medical Engineering	Beijing, China	Pancreas
JC 200	Chongqing Haifu (HIFU) Medical Technology Co., LTD	Chongqing, China	Uterus, Liver, Bones, Breast
HIFUNIT9000	Shanghai A&S Co., LTD	Shanghai, China	Pancreas
Pro2008	Shenzhen PRO-HIFU Medical Tech. Co., LTD	Shenzhen, China	Uterus
Ablatherm	EDAP-TMS	Lyon, France	Prostate
Focal One			

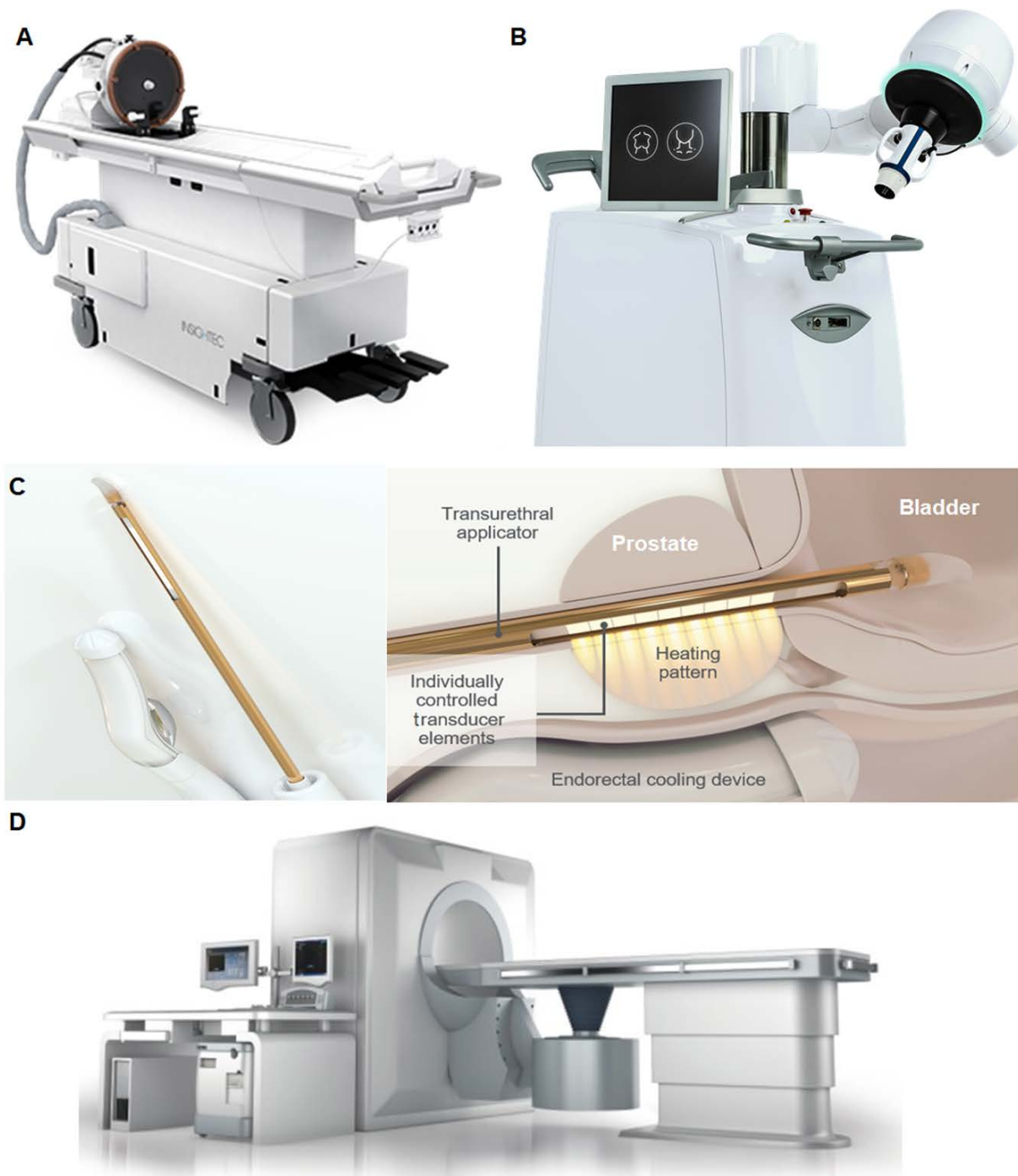


FIGURE 3. Clinically approved HIFU systems. **A** MRgHIFU system for neurological application (INSIGHTEC, Israel). The patient table includes the focused ultrasound transducer mounted on a mechanical positioning unit with an MR-compatible head frame that can be docked to the MR scanner. **B** EchoPulse® USgHIFU system (Theraclion, France) for treatment of thyroid nodules and breast fibroadenomas. **C** Transurethral MRgHIFU ablation system for prostate cancer (Profound Medical). **D**

USgHIFU system (HAIFU, China) for solid tumor ablation of all types of soft tissue. ©By courtesy of INSIGHTEC THERACLION, Profound Medical and Chongqing HAIFU.

INNOVATIVE APPLICATIONS OF IMAGE-GUIDED FOCUSED ULTRASOUND

In addition to image-guided HIFU ablation described above, focused ultrasound (FUS) at various intensities offers advantages in many other potential applications. The following section presents selected preclinical and clinical studies of FUS as a single or adjuvant therapy.

Histotripsy

As mentioned previously, dense energetic bubble clouds can be produced at the focus point by very short, infrequent, high amplitude bursts of acoustic waves that mechanically fractionate the tissue into subcellular components in histotripsy (36). Compared to thermal applications, histotripsy avoids overheating and the heat-sink effect in the targeted tissues, and the resorption of tissue fragments is easier after treatment.

Several recent studies showed the feasibility of using histotripsy to create precise lesions at the desired location, such as the liver, prostate, or brain (36). Notably, lesions can be created through the ribs safely throughout the entire liver (37). The first-in-human study using cavitation histotripsy for the treatment of prostate enlargement was reported in 2018. An improvement of lower urinary tract symptoms was observed with no intraoperative side effects. However, the treatment outcome was not as significant as expected, due to the technical limitations of the FUS device (38). The development of a precisely controlled histotripsy FUS system is necessary.

Histotripsy is a neurosurgical option (39), in which lesions with a dimension of up to 1 cm are created in the porcine cortex without thermal-induced damage to the surrounding neurons. Moreover, histotripsy carries the potential to overcome the limitations of current thrombolytic drugs as well as shortening the treatment time. *In vitro* and *in vivo* experiments have shown that FUS histotripsy

thrombolysis can cause a direct mechanical breakdown of clots and achieve blood flow restoration noninvasively (40).

FUS-Mediated Drug Delivery

The systemic toxicity of chemotherapy is the main challenge in clinical oncology and may induce adverse effects such as hair loss, anemia, nausea, and vomiting. The encapsulation of chemotherapeutic drugs in carriers and/or the triggering of drug delivery in the target tissue with external physical stimulation have been considered to improve treatment efficiency and reduce adverse effects. Based on mechanical and thermal mechanisms, FUS-mediated targeted drug delivery has become a topic of intensive research in the last 20 years. The drug carriers can be opened *in situ* and allow controlled drug release in specific regions with FUS exposure, and the permeability of the cell membrane and the drug uptake can be enhanced as well (41). A preclinical study reported on the combination of the chemotherapeutic agent gemcitabine and showed that FUS treatment led to a reduction in tumor growth compared to a single treatment in the xenograft pancreatic cancer model (42).

In addition to chemotherapeutic drugs, ultrasound-mediated gene delivery provides a new strategy for cancer treatment. The typical ultrasound parameters used for gene delivery are frequencies of 1–2 MHz, intensities of 0.1–3 W/cm² with a short duration of 2–8 s, and ultrasound contrast agent microbubbles are usually added to enhance the sonoporation effect (43). Noroozian *et al.* (44) demonstrated the FUS-mediated recombinant adeno-associated viral vector across the blood–brain barrier into the brain parenchyma, which resulted in efficient gene transduction and expression in both mouse and rat models.

A single-center phase 1 trial (NCT02181075) was conducted in the UK to analyze the safety and feasibility of FUS-hyperthermia-triggered doxorubicin delivery from thermosensitive liposomes (45). Thermosensitive liposomal doxorubicin was administered by intravenous infusion, followed by FUS exposure at a single target liver tumor. The concentration of doxorubicin inside the target tumor was increased by 3.7-fold immediately after FUS treatment compared to the group without FUS.

FUS Supporting Radiation Therapy

Radiation therapy (RT) is one of the most commonly used treatment modalities in clinic. Various biological mechanisms are involved in enhancing the anti-tumor effects of RT, including the inhibition of DNA damage repair, induction of apoptosis, and change of tumor microenvironment (46). A few clinical studies have shown that FUS is a sensitizer of RT in different cancers including head and neck, breast, prostate, and central nervous system malignancies (3).

A phase I study by Chu *et al.* (47) reported the combined treatment of MRgHIFU hyperthermia, RT and chemotherapy for recurrent rectal cancer. Patients received daily fractionated RT (total dose 30.6 Gy) and oral capecitabine. HIFU-hyperthermia was performed at a mean temperature of 42.5 °C for 30 min immediately before RT on days 1, 8, and 15. No intraoperative complications, serious adverse effects, or unexpected tissue damage attributed to HIFU-hyperthermia were observed, showing the safety and treatment feasibility. Another phase II study reported a 7-year overall survival rate of 94% in advanced prostate cancer patients after combined treatment of transrectal ultrasound-hyperthermia, RT, and androgen suppression (48).

A better understanding of ultrasound radiosensitization mechanisms is necessary, although benefits have been shown in several clinical studies. The significant radioadditive effect of FUS in prostate cancer was demonstrated in our *in vitro* study (49,50). It is critical to optimize the combination treatment protocols to increase the treatment efficiency in terms of the treatment sequences, interval time, thermal dose, and radiation dose. The integration of FUS into RT and the administration of both treatments simultaneously may improve the radiosensitization effect further.

FUS-Mediated Immunotherapy

Immunotherapy has changed cancer treatment strategies, aiming to improve the anti-tumor immune response and directly kill cancer cells (51). The immune system is activated or the activation process is

boosted by immunotherapeutic agents such as checkpoint inhibitors to attack cancer cells through natural mechanisms and avoid relative side effects.

FUS provides the possibility to deliver immunotherapy agents, and FUS administration, especially the mechanisms of cavitation, is considered a stimulator for the immune system (52). Eranki et al. (53) reported that the mechanical fractionation of neuroblastoma tumors using HIFU significantly increases cellular immunity, and the combination of HIFU and checkpoint inhibitors induces systemic immunity and dramatically enhances survival. More experimental and clinical evidence of FUS-induced immune effects was systematically reviewed by van den Bijgaart *et al.* (54). However, the safety of FUS-induced immune therapy is the main obstacle for clinical translation because of tumor heterogeneity. The underlying mechanisms of the interactions between ultrasound and cells are of vital importance and a better understanding is needed before clinical trials.

Neuromodulation by Low-Intensity FUS

Transcranial FUS application in neurological diseases is of particular interest. The potential indications include Alzheimer's disease, depression, obsessive-compulsive disorder, epilepsy, and Huntington's disease. FUS-mediated neuromodulation is performed at low intensities and for short durations (55). Mechanical effects are considered the main driver for neuron stimulation, since the temperature increase is limited at the target.

Storz Medical has introduced the CE-marked system Neurolith® for the single-pulse-wave treatment of Alzheimer's disease with promising initial clinical results (56). Low-intensity FUS with short bursts is a promising method for the safe stimulation or inhibition of neurons in future clinical neurological applications and will not require hair shaving for the patients. A new system clinical FUS operating at diagnostic sound pressure for neuromodulation has been developed in collaboration by the Innovation Center Computer Assisted Surgery and the Fraunhofer IBMT (Sulzbach, Germany) and is currently being validated at the Max Planck Institute for Cognitive and Neurosciences in Leipzig. The preliminary results were reported by Villringer *et al.* in the first Focused Ultrasound Neuromodulation Symposium in Oxford

in 2019. Further work is necessary to explore the ultrasound parameters and to develop targeted neuromodulation methods in different brain regions.

NOVEL TECHNIQUES FOR POTENTIAL IMAGE-GUIDED HIFU APPLICATIONS

Various studies have been conducted to integrate multi-functional imaging modalities into the FUS system to improve the safety, treatment efficiency, and accuracy of the outcome assessment. PET/MRI was also reported to detect the local recurrence of prostate cancer patients after HIFU ablation, which is not detectable by MR imaging. Moreover, PET/MRI images could be used for the target optimization of a secondary HIFU ablation and could improve patient survival (57). Novel tracers, such as the prostate-specific membrane antigen, have shown promising results in patients for the detection of prostatic cancer using PET/MRI (58). In combination with HIFU, this may allow for a “one-stop-shop” treatment towards focal therapy.

A robotic assistance system was previously integrated into an MR scanner to provide precise and reproducible instrument positioning (59). To realize precise FUS positioning under PET/MRI imaging guidance, we are working on the integration of a robotic arm system with an MR-compatible FUS transducer into the clinical PET/MRI scanner (Figure 4) (60). This new concept expands the application field of image-guided FUS interventions, may provide clinical feasibility, and will allow precise treatment in the near future.

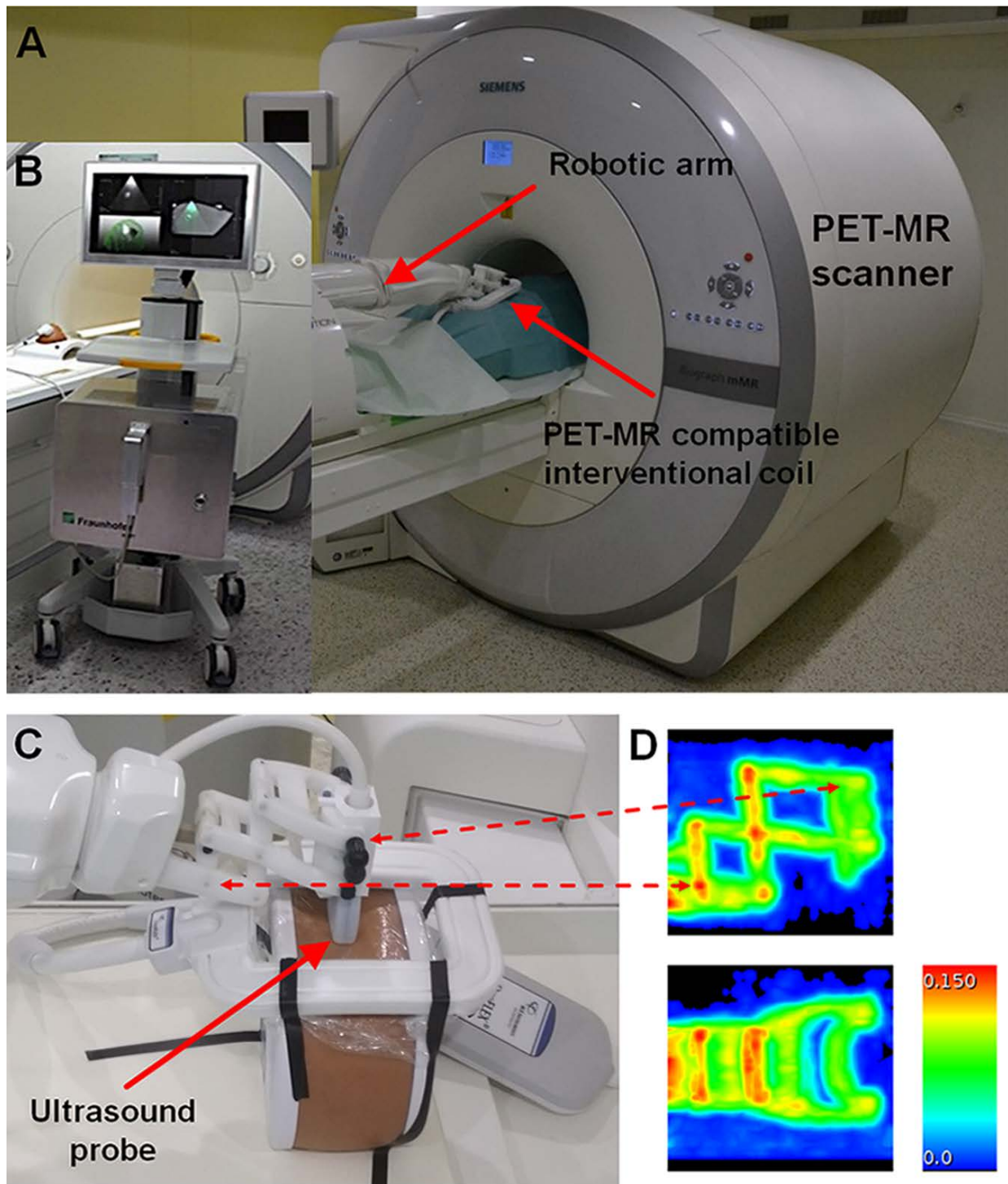


FIGURE 4. Integration of the INNOMOTION robotic arm (InnoMedic GmbH, Germany) into the Biograph PET/MRI scanner (Siemens Healthineers). **A** The robotic arm was modified to fit into the PET/MRI system holding an ultrasound imaging probe. **B** MR-compatible focused ultrasound (FUS) system Diphos (Fraunhofer IBMT) can be integrated into the PET/MRI scanner. **C** Three-dimensional-printed adaptor and

fixation parts were manufactured to hold an ultrasound transducer. **D** Attenuation map of the robotic arm visualized by 2 perpendicular maximum-intensity projections of PET annihilation photons (in 1/cm) with linear attenuation coefficient of 511keV, obtained by stand-alone PET scanner equipped with 68Ge-/68Ga rod sources.

CONCLUSION

Imaged-guided HIFU is a promising noninvasive, non-access method applied in the clinic that has been proven to be efficient and safe in several studies. It has been approved in all major markets around the world for the treatment of uterine fibroids, bone metastases, liver tumors, brain, and prostate cancer. The advantages of the method are its noninvasiveness, absence of ionizing radiation, comparatively low complication rates, and side effect rate with a correspondingly low impairment of quality of life. With a transcranial HIFU system, the treatment of essential tremors and Parkinson-induced tremors is clinically approved, and studies are currently underway with promising initial results in neurological diseases. The potential of HIFU has been demonstrated for various medical applications to improve other treatment modalities such as chemotherapy and radiation therapy and to support drug delivery. Imaging innovation together with HIFU treatment may provide a new strategy for future clinical applications.

NOTEWORTHY

- HIFU ablation has been used in the clinic for the noninvasive treatment of various diseases under ultrasound or MR-imaging guidance. (Page 8)
- The combination of HIFU with other therapies showed promising advances in recent preclinical and clinical studies. (Page 18)
- The integration of the multi-functional imaging guidance modality into HIFU is required for precise treatment and accurate treatment outcome evaluation (Page 22)

DISCLOSURE

No potential conflicts of interest relevant to this article exist.

ACKNOWLEDGEMENT

The work described was supported by research grants funded by the German Ministry of Science and Technology BMBF “SONO-RAY” project (03Z1L511). The Depts of Nuclear Medicine and Radiation Therapy of the Leipzig University Hospital are mentioned with gratitude for supporting some of the work mentioned. Further results will be published elsewhere. Saxon Incubator for Clinical Translation (SIKT) and Fraunhofer Institute for Cell Therapy and Immunology (Fraunhofer IZI) are mentioned with gratitude for supporting the preclinical experiments.

REFERENCES

1. Kennedy JE. High-intensity focused ultrasound in the treatment of solid tumours. *Nat Rev Cancer*. 2005;5:321-327.
2. Siedek F, Yeo SY, Heijman E, et al. Magnetic resonance-guided high-intensity focused ultrasound (MR-HIFU): technical background and overview of current clinical applications (part 1). *Rofo*. 2019;191:522-530.
3. Zhu L, Altman MB, Laszlo A, et al. Ultrasound hyperthermia technology for radiosensitization. *Ultrasound Med Biol*. 2019;45:1025-1043.
4. Jolesz FA. MRI-guided focused ultrasound surgery. *Annu Rev Med*. 2009;60:417-430.
5. Izadifar Z, Izadifar Z, Chapman D, Babyn P. An introduction to high intensity focused ultrasound: Systematic review on principles, devices, and clinical applications. *J Clin Med*. 2020;9:460.
6. McWilliams JP, Lee EW, Yamamoto S, Loh CT, Kee ST. Image-guided tumor ablation: Emerging technologies and future directions. *Semin Intervent Radiol*. 2010;27:302-313.
7. Prentice P, Cuschierp A, Dholakia K, Prausnitz M, Campbell P. Membrane disruption by optically controlled microbubble cavitation. *Nat Phys*. 2005;1:107-110.
8. Rosenthal I, Sostaric JZ, Riesz P. Sonodynamic therapy - a review of the synergistic effects of drugs and ultrasound. *Ultrason Sonochem*. 2004;11:349-363.
9. Orsi F, Arnone P, Chen WZ, Zhang LA. High intensity focused ultrasound ablation: a new therapeutic option for solid tumors. *J Cancer Res Ther*. 2010;6:414-420.

10. Orsi F, Monfardini L, Bonomo G, Krokidis M, Della Vigna P, Disalvatore D. Ultrasound guided high intensity focused ultrasound (USgHIFU) ablation for uterine fibroids: do we need the microbubbles? *Int J Hyperthermia*. 2015;31:233-239.
11. Samset E. Temperature mapping of thermal ablation using MRI. *Minimally Invasive Therapy & Allied Technologies*. 2006;15:36-41.
12. Stewart EA. Clinical practice. uterine fibroids. *N Engl J Med*. 2015;372:1646-1655.
13. Wu G, Li R, He M, et al. A comparison of the pregnancy outcomes between ultrasound-guided high-intensity focused ultrasound ablation and laparoscopic myomectomy for uterine fibroids: a comparative study. *Int J Hyperthermia*. 2020;37:617-623.
14. Duc NM, Keserci B. Review of influential clinical factors in reducing the risk of unsuccessful MRI-guided hifu treatment outcome of uterine fibroids. *Diagn Interv Radiol*. 2018;24:283-291.
15. Hopfner F, Deuschl G. Managing essential tremor. *Neurotherapeutics*. 2020;17:1603-1621.
16. Elias WJ, Lipsman N, Ondo WG, et al. A randomized trial of focused ultrasound thalamotomy for essential tremor. *N Engl J Med*. 2016;375:730-739.
17. Park YS, Jung NY, Na YC, Chang JW. Four-year follow-up results of magnetic resonance-guided focused ultrasound thalamotomy for essential tremor. *Mov Disord*. 2019;34:727-734.
18. Durante C, Costante G, Lucisano G, et al. The natural history of benign thyroid nodules. *JAMA*. 2015;313:926-935.
19. Lang BHH, Wu ALH. High intensity focused ultrasound (HIFU) ablation of benign thyroid nodules - a systematic review. *J Ther Ultrasound*. 2017;5:11.
20. Esnault O, Franc B, Menegaux F, et al. High-intensity focused ultrasound ablation of thyroid nodules: first human feasibility study. *Thyroid*. 2011;21:965-973.
21. Prakash PS, Oh HB, Tan WB, Parameswaran R, Ngiam KY. The efficacy and safety of high-intensity focused ultrasound (HIFU) therapy for benign thyroid nodules-a single center experience from singapore. *World J Surg*. 2019;43:1957-1963.
22. Hahn M, Fugunt R, Schoenfish B, et al. High intensity focused ultrasound (HIFU) for the treatment of symptomatic breast fibroadenoma. *Int J Hyperthermia*. 2018;35:463-470.

23. Barsouk A, Padala SA, Vakiti A, et al. Epidemiology, staging and management of prostate cancer. *Med Sci (Basel)*. 2020;8.
24. Valerio M, Cerantola Y, Eggener SE, et al. New and established technology in focal ablation of the prostate: A systematic review. *Eur Urol*. 2017;71:17-34.
25. Eggener S, Koch M, Penson D, et al. Pivotal trial of MRI-guided transurethral ultrasound ablation in men with localized prostate cancer: two-year follow-up. *J Urol*. 2020;203:e369-e369.
26. Bonekamp D, Wolf MB, Roethke MC, et al. Twelve-month prostate volume reduction after MRI-guided transurethral ultrasound ablation of the prostate. *Eur Radiol*. 2019;29:299-308.
27. Chin JL, Billia M, Relle J, et al. Magnetic resonance imaging-guided transurethral ultrasound ablation of prostate tissue in patients with localized prostate cancer: a prospective phase 1 clinical trial. *Eur Urol*. 2016;70:447-455.
28. Klotz L, Pavlovich CP, Chin J, et al. Magnetic resonance imaging-guided transurethral ultrasound ablation of prostate cancer. *J Urol*. 2021;205:769-779.
29. Ganzer R, Hadaschik B, Pahernik S, et al. Prospective multicenter phase II study on focal therapy (hemablation) of the prostate with high intensity focused ultrasound. *J Urol*. 2018;199:983-989.
30. Loi M, Nuyttens JJ, Desideri I, Greto D, Livi L. Single-fraction radiotherapy (SFRT) for bone metastases: Patient selection and perspectives. *Cancer Manag Res*. 2019;11:9397-9408.
31. Hurwitz MD, Ghanouni P, Kanaev SV, et al. Magnetic resonance-guided focused ultrasound for patients with painful bone metastases: Phase III trial results. *J Natl Cancer Inst*. 2014;106.
32. Napoli A, Anzidei M, Marincola BC, et al. Primary pain palliation and local tumor control in bone metastases treated with magnetic resonance-guided focused ultrasound. *Invest Radiol*. 2013;48:351-358.
33. Carrato A, Falcone A, Ducreux M, et al. A systematic review of the burden of pancreatic cancer in europe: real-world impact on survival, quality of life and costs. *J Gastrointest Cancer*. 2015;46:201-211.
34. Marinova M, Huxold HC, Henseler J, et al. Clinical effectiveness and potential survival benefit of US-guided high-intensity focused ultrasound therapy in patients with advanced-stage pancreatic cancer. *Ultraschall Med*. 2019;40:625-637.
35. Marinova M, Feradova H, Gonzalez-Carmona MA, et al. Improving quality of life in pancreatic cancer patients following high-intensity focused ultrasound (HIFU) in two european centers. *Eur Radiol*. 2021;10.1007/s00330-020-07682-z.

36. Khokhlova VA, Fowlkes JB, Roberts WW, et al. Histotripsy methods in mechanical disintegration of tissue: towards clinical applications. *Int J Hyperthermia*. 2015;31:145-162.
37. Vlasisavljevic E, Owens G, Lundt J, et al. Non-invasive liver ablation using histotripsy: preclinical safety study in an in vivo porcine model. *Ultrasound Med Biol*. 2017;43:1237-1251.
38. Schuster TG, Wei JT, Hendlin K, Jahnke R, Roberts WW. Histotripsy treatment of benign prostatic enlargement using the Vortex rx system: Initial human safety and efficacy outcomes. *Urology*. 2018;114:184-187.
39. Sukovich JR, Cain CA, Pandey AS, et al. In vivo histotripsy brain treatment. *J Neurosurg*. 2018;10.3171/2018.4.JNS172652:1-8.
40. Shi A, Lundt J, Deng Z, et al. Integrated histotripsy and bubble coalescence transducer for thrombolysis. *Ultrasound Med Biol*. 2018;44:2697-2709.
41. Jain A, Tiwari A, Verma A, Jain SK. Ultrasound-based triggered drug delivery to tumors. *Drug Deliv Transl Res*. 2018;8:150-164.
42. Park EJ, Ahn YD, Lee JY. In vivo study of enhanced chemotherapy combined with ultrasound image-guided focused ultrasound (USgFUS) treatment for pancreatic cancer in a xenograft mouse model. *Eur Radiol*. 2018;28:3710-3718.
43. Yoon CS, Park JH. Ultrasound-mediated gene delivery. *Expert Opin Drug Deliv*. 2010;7:321-330.
44. Noroozian Z, Xhima K, Huang Y, et al. MRI-guided focused ultrasound for targeted delivery of raav to the brain. *Methods Mol Biol*. 2019;1950:177-197.
45. Lyon PC, Gray MD, Mannaris C, et al. Safety and feasibility of ultrasound-triggered targeted drug delivery of doxorubicin from thermosensitive liposomes in liver tumours (tardox): A single-centre, open-label, phase 1 trial. *Lancet Oncol*. 2018;19:1027-1039.
46. Rao W, Deng ZS, Liu J. A review of hyperthermia combined with radiotherapy/chemotherapy on malignant tumors. *Crit Rev Biomed Eng*. 2010;38:101-116.
47. Chu W, Huang Y, Pichardo S, et al. A phase i study of mr-hifu hyperthermia (HT) with radiation (RT) and chemotherapy (CT) for recurrent rectal cancer. *J Glob Oncol*. 2019;5:78-78.
48. Hurwitz MD, Hansen JL, Prokopios-Davos S, et al. Hyperthermia combined with radiation for the treatment of locally advanced prostate cancer: long-term results from dana-farber cancer institute study 94-153. *Cancer*. 2011;117:510-516.

49. Hu S, Zhang X, Unger M, Patties I, Melzer A, Landgraf L. Focused ultrasound-induced cavitation sensitizes cancer cells to radiation therapy and hyperthermia. *Cells*. 2020;9.
50. Zhang X, Bobeica M, Unger M, et al. Focused ultrasound radiosensitizes human cancer cells by enhancement of DNA damage. *Strahlentherapie und Onkologie*. 2021;10.1007/s00066-021-01774-5.
51. Riley RS, June CH, Langer R, Mitchell MJ. Delivery technologies for cancer immunotherapy. *Nat Rev Drug Discov*. 2019;18:175-196.
52. Mauri G, Nicosia L, Xu Z, et al. Focused ultrasound: Tumour ablation and its potential to enhance immunological therapy to cancer. *Br J Radiol*. 2018;91:20170641.
53. Eranki A, Srinivasan P, Ries M, et al. High-intensity focused ultrasound (HIFU) triggers immune sensitization of refractory murine neuroblastoma to checkpoint inhibitor therapy. *Clin Cancer Res*. 2020;26:1152-1161.
54. van den Bijgaart RJ, Eikelenboom DC, Hoogenboom M, Futterer JJ, den Brok MH, Adema GJ. Thermal and mechanical high-intensity focused ultrasound: Perspectives on tumor ablation, immune effects and combination strategies. *Cancer Immunol Immunother*. 2017;66:247-258.
55. Naor O, Krupa S, Shoham S. Ultrasonic neuromodulation. *J Neural Eng*. 2016;13:031003.
56. Beisteiner R, Matt E, Fan C, et al. Transcranial pulse stimulation with ultrasound in alzheimer's disease-a new navigated focal brain therapy. *Adv Sci*. 2020;7:1902583.
57. Burger IA, Muller J, Donati OF, et al. (68)Ga-PSMA-11 PET/MR detects local recurrence occult on mpMRI in prostate cancer patients after HIFU. *J Nucl Med*. 2019;60:1118-1123.
58. Eiber M, Nekolla SG, Maurer T, Weirich G, Wester HJ, Schwaiger M. (68)Ga-PSMA PET/MR with multimodality image analysis for primary prostate cancer. *Abdom Imaging*. 2015;40:1769-1771.
59. Melzer A, Gutmann B, Remmele T, et al. Innomotion for percutaneous image-guided interventions: principles and evaluation of this MR- and CT-compatible robotic system. *IEEE Eng Med Biol Mag*. 2008;27:66-73.
60. Berger J, Unger M, Landgraf L, Melzer A. Evaluation of an IEEE 11073 sdc connection of two KUKA robots towards the application of focused ultrasound in radiation therapy. *Current Directions in Biomedical Engineering*. 2019;5:149.